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# QUANTITATIVE ASSESSMENT OF STRENGTH AND FATIGUE IN PATIENTS WITH MYASTHENIA GRAVIS

M. Caitlin J. Symonette Western University

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#### **QUANTITATIVE ASSESSMENT OF STRENGTH AND FATIGUE IN PATIENTS WITH MYASTHENIA GRAVIS**

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(Spine title: Strength and Fatigue in Patients with Myasthenia Gravis)

(Thesis format: Integrated-Article)

by

M. Caitlin J. Symonette

Graduate Program in Kinesiology

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A thesis submitted in partial fulfillment of the requirements for the degree of Master of Science

Faculty of Graduate Studies The University of Western Ontario London, Ontario, Canada

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#### THE UNIVERSITY OF WESTERN ONTARIO FACULTY OF GRADUATE STUDIES

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#### **M. CaitIin J. Symonette**

entitled:

## **Quantitative Assessment of Strength and Fatigue in Patients with Myasthenia Gravis**

Is accepted in partial fulfilment of the requirements for the degree of Master of Science

Date Chair of Thesis Examination Board

#### **ABSTRACT**

The objective of this thesis was to quantify, by direct measurement of muscle force, the strength and fatigue of patients with myasthenia gravis (MG). MG is characterized by fatigable muscle weakness resulting from impaired neuromuscular transmission.

A maximal voluntary isometric contraction protocol of shoulder abductors was used in conjunction with conventional fatigue and disease severity instruments. Results from patients with (D-MG) and without. decrement (ND-MG) on repetitive nerve stimulation (RNS) were compared to controls.

Patients with MG reported experiencing greater fatigue than controls. Muscle strength was the lowest in the D-MG group followed by the ND-MG group and controls, respectively. Surprisingly, normalized shoulder abduction fatigue and recovery values did not differ between patients with MG and controls.

Greater experienced fatigue in MG may correspond to confounding variables such as physical inactivity. In addition, decrement upon RNS, appears to relate best to disease severity and muscle weakness but not to fatigue in this population.

**Keywords:** myasthenia gravis, repetitive nerve stimulation, fatigue, weakness, isometric force, deltoid muscle, quantitative myasthenia gravis score, manual muscle testing, myasthenia gravis fatigue scale

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#### **LIST OF ABBREVIATIONS**

**ACh-** acetylcholine **AChE-** acetylcholinesterase **AChR-** acetylcholine receptor **ADL-** activities of daily living ANOVA- analysis of variance **BMI-** body mass index **Ca2+-** calcium **CAF -** central activation failure **CNS-** central nervous system **CMAP-** compound muscle action potential **D-MG -** decrementing myasthenia gravis **EAMG -** experimental autoimmune myasthenia gravis **EPP-** end-plate potential **MFAP-** muscle fiber action potential **MG-** myasthenia gravis **MG-ADL-** myasthenia gravis- activities of daily living scale **MGFS-** myasthenia gravis fatigue scale **MIR-** main immunogenic region **MMT-** manual muscle testing **MN-** motor neuron **MS-** multiple sclerosis **MU-** motor unit **MVC -** maximal voluntary contraction **MVIC-** maximal voluntary isometric contraction **NMD -** neuromuscular disorders **ND-MG -** non-decrementing myasthenia gravis **NMJ-** neuromuscular jimction **NMT-** neuromuscular transmission **NpAmp-** negative peak amplitude **QMG-** quantitative myasthenia gravis score **RNS-** repetitive nerve stimulation **SD-** standard deviation **SFEMG-** single fiber electromyography **VAS-** visual analogue scale **VGCC-** voltage gated calcium channels **VGNa+ channels-** voltage gated sodium channels

#### **GLOSSARY OF TERMS**

**Acetylcholine (ACh) -** neurotransmitter at the neuromuscular junction

**Acetylcholinesterase (AChE) -** enzyme responsible for hydrolyzing free acetylcholine within the neuromuscular synapse into choline and acetate

**Acetylcholine receptor (AChR) -** integral membrane receptor of the muscle end-plate which responds to binding of two acetylcholine molecules by undergoing a conformational change which promotes the entry of cations into the muscle end-plate

**Compound muscle action potential (CMAP) -** surface detected potential representing the summation of all the muscle fiber action potentials within a muscle following supramaximal stimulation of the appropriate motor nerve

**End-plate potential (EPP) -** partial post-synaptic cell depolarization produced by opening of cation channels at the muscle end-plate

**Fatigue** – deficit in a muscle or muscle groups ability to sustain a given or required force over time

**Jitter** – variability in neuromuscular transmission time across different neuromuscular junctions belonging to a single motor unit

**Muscle end-plate -** region of muscle, characterized by <sup>a</sup> high density of neuromuscular junctions, which is responsible for the initiation of muscle fiber action potentials

**Muscle fiber action potential (MFAP) -** action potential across the muscle fiber sarcolemma and T-tubules which initiates a muscle contraction

**Myasthenia gravis (MG) -** an autoimmune disease characterized by fatigable skeletal muscle weakness resulting from impaired neuromuscular transmission

**Myasthenia gravis- activities of daily living scale (MG-ADL) -** <sup>a</sup> Likert scale that measures the impact of myasthenia gravis on activities of daily living as an indictor of disease severity

**Myasthenia gravis fatigue scale (MGFS) -** self-report questionnaire examining three subscales of fatigue including perception of fatigue, task avoidance behaviors, and observable motor signs

**Manual muscle testing (MMT) -** clinical evaluation of muscle strength developed by the medical research council (MRC)

**Maximal voluntary isometric contraction (MVIC) -** maximal effort voluntary contraction where the joint angle remains constant during the contraction

**Negative-peak amplitude (NpAmp) -** <sup>a</sup> measurement relating to the change in recorded millivolts from baseline to the peak of the negative phase of <sup>a</sup> surface detected compound muscle action potential

**Neuromuscular junction (NMJ) -** <sup>a</sup> specialized synapse between <sup>a</sup> motor neuron and <sup>a</sup> muscle end-plate .

**Peak torque -** the maximum production of force about <sup>a</sup> vector (the dynamometer arm) for <sup>a</sup> single contraction, measured in newton-meters (Nm)

**Quantitative myasthenia gravis score (QMG) -** <sup>a</sup> clinical instrument used to assess disease severity by testing the strength of thirteen different muscle groups

**Repetitive nerve stimulation (RNS) -** an electrodiagnostic test for disorders of neuromuscular transmission which involves recording various parameters of <sup>a</sup> compound muscle action potential following repeated supramaximal stimulations of the appropriate motor nerve

**Sensitivity -** the probability of correctly detecting the presence of a given abnormality

**Single fiber electromyography (SFEMG) -** an electrodiagnostic test for disorders of neuromuscular transmission where <sup>a</sup> needle electrode is inserted into the muscle to examine for jitter and blocking

**Specificity -** the probability of correctly detecting the absence of <sup>a</sup> given abnormality

**Visual analogue scale (VAS) -** <sup>a</sup> research instrument designed to measure an attribute that is best illustrated by a continuum of values versus discrete points

**Weakness-** loss of strength within a given muscle independent of previous work or activity

#### **CHAPTER <sup>1</sup>**

#### **NEUROMUSCULAR FATIGUE AND WEAKNESS**

#### **1 .0 GENERAL INTRODUCTION**

#### **1 .0.1 Myasthenia Gravis**

Myasthenia Gravis (MG) is <sup>a</sup> post-synaptic neuromuscular junction (NMJ) disorder characterized by fatigable skeletal muscle weakness exacerbated with activity and improved with rest<sup>23,33,25</sup>. The asymmetric and varied presentation of affected muscle groups creates unique challenges in the diagnosis and treatment of  $\text{MG}^{25,33}$ . Ocular, bulbar, and proximal muscle groups are most commonly involved<sup>8,33,5</sup> and individuals indiscriminate of race, age, or gender may present with symptoms of  $MG<sup>24,33</sup>$ . Although mortality rates have declined to less than five percent, contemporary prevalence rates continue to advance towards 1 in  $5,000$  people<sup>20,28</sup>. With the aid of animal and human experiments, the site and mechanism of fatigue in MG have been identified as neuromuscular transmission (NMT) failure across <sup>a</sup> specialized synapse called the  $NMI<sup>23,25,20,33</sup>$ 

#### **1 .0.2 The Neuromuscular Junction**

Voluntary movement generated by mammalian skeletal muscle is the product of an intricate orchestration of central and peripheral events. The motor unit (MU), comprised of a single  $\alpha$ - motor neuron (MN) and the muscle fibers its' axon innervates, is responsible for translating signals from the central nervous system (CNS) into meaningful motor responses<sup>19,32,8</sup>. Each MN cell body, located in the anterior horn of the spinal column<sup>8</sup>, projects a myelinated motor axon to a specific muscle<sup>8</sup>. Once the motor axon enters the muscle, it loses its myelin sheath and divides into multiple terminai

 $2^2$   $T1$ branches forming a NMJ with each individual muscle fiber<sup>32</sup>. The NMJ is a specialized synapse within the MU (Figure 1.1).

Action potentials from MNs are conveyed via the neurotransmitter acetylcholine (ACh) across the NMJ to the motor end-plate of the muscle to initiate the series of events that eventually lead to contraction. When an action potential in the MN reaches the nerve terminal, it stimulates voltage gated calcium channels (VGCC) to open<sup>5,19</sup>. The influx of positive charge results in the exocytosis of ACh from vesicles into the primary synaptic  $c$ left<sup>19</sup>. Each ACh vesicle contains a discrete amount of ACh molecules referred to as quanta<sup>19,21</sup>. In the pre-synaptic terminal, ACh quanta are organized into immediately releasable, mobilizable, and reserve stores<sup>19,5,8</sup>. Only a modest number of quanta are available for immediate release from the active zones of the pre-synaptic membrane. As the initial stores deplete, the mobilizable stores are engaged to release additional ACh quanta<sup>5,8</sup>. Once in the synaptic cleft, ACh rapidly diffuses across the 50 nm space to interact with the nicotinic ACh receptors (AChR) located on the crests of the junctional folds of the post-synaptic muscle membrane<sup>5,19,33</sup>. ACh-AChR interactions open the AChR channel pores allowing an influx of cations, predominately Na+, into the postsynaptic muscle cell<sup>5,33</sup>. In addition to increasing surface area, the narrow junctional folds act to create <sup>a</sup> high resistance path to current flow facilitating the activation of voltage gated sodium (VG Na+) channels concentrated at the base of the folds<sup>8,19</sup>.

Each ACh quantum released results in approximately <sup>a</sup> 1 mV change of postsynaptic membrane potential<sup>5</sup>. If the local depolarizations, so called end-plate potentials (EPP), reach <sup>a</sup> certain threshold an all-or-none muscle fiber action potential (MFAP) occurs<sup>5,33,32</sup>. Each MFAP travels bi-directionally along the muscle fiber stimulating subsequent events which generate a muscle contraction<sup>7</sup>. The safety factor responsible for preserving signal transmission across the NMJ is protected by an excess of ACh-AChR. interactions above the amount required for a threshold response<sup>23</sup>. After closure of the AChR pore, ACh either diffuses away from the NMJ or is hydrolyzed by the enzyme

#### **1 .0.3 Neuromuscular Junction Pathophysiology in Myasthenia Gravis**

subsequent events which generate a muscle contraction<sup>7</sup>. The safety fact<br>preserving signal transmission across the NMJ is protected by an exce<br>interactions above the amount required for a threshold response<sup>23</sup>. Af<br>AChR Impaired NMT is the result of a T-cell dependent autoimmune attack on various epitopes of the skeletal muscle end-plate region<sup>39</sup>. One of the putative epitope regions is the main immunogenic region (MIR) of the  $\alpha$ -subunit of AChRs embedded in the postsynaptic membrane<sup>39,18,20</sup>. The binding of two ACh molecules, released from the MN terminal, to AChR  $\alpha$ -subunits is required to initiate a cascade of events resulting in muscle contraction<sup>39,33,23</sup>. When the NMT is blocked at the postsynaptic membrane, as is the case in MG, the corresponding muscle fibers fail to contract resulting in weakness and fatigue $33$ .

Three principal mechanisms have been proposed to explain how anti-AChR antibodies operate at the NMJ. The first mechanism by which anti-AChR antibodies may compromise NMT is by interfering, either competitively or non-competitively, with the ability of ACh to bind to the  $\alpha$ -subunit of the AChR<sup>39,33</sup>. In healthy NMJs, AChRs are continually being replaced and have <sup>a</sup> half-life of approximately 8-11 days before they are internalized and degraded<sup>41</sup>. However due to clustering of AChRs on the crests of junctional folds, anti-AChR antibodies are able to easily cross-link adjacent  $AChRs<sup>39,33</sup>$ . The second mechanism, cross-linking receptors, results in faster internalization kinetics and lower steady-state AChR concentrations<sup>33</sup>. The third proposed mechanism reveals



Figure 1.1. Schematic of an intact neuromuscular junction. The pre-synaptic nerve terminai contains synaptic vesicles and voltage-gated calcium channels (VGCC). Free acetylcholine (ACh) and the enzyme acetylcholinesterase (AChE) are depicted in the primary synaptic cleft. Acetylcholine receptors (AChR) are located on the crests of postsynaptic junctional folds of the muscle endplate, where voltage-gated sodium (VG Na+) channels are concentrated in the troughs. (Adapted from Nicolle MW: Myasthenia Gravis. Neurologist 2002; 8 (1): 2-21.)<sup>33</sup>

potentially one of the most detrimental and long-term consequences of anti-AChR antibodies. Anti-AChR antibodies are able to activate the complement system<sup>39</sup>. Once activated, the complement system forms <sup>a</sup> membrane-attack complex through <sup>a</sup> network of associated proteins which results in the destruction of the muscle end-plate<sup>39,33</sup>. Overall, each antibody mechanism compromises an important safety factor for NMT by impeding the actions of ACh or reducing the number of available AChRs at the muscle end-plate.

Through elucidating the complex pathophysiology of MG, investigators have improved the prognosis and available treatment options to effectively manage the disease<sup>25,7,33</sup>. For example, the development of AChE inhibitor medications, such as pyridostigmine bromide (Mestinon®), has proven successful in the symptomatic treatment of  $MG^{23,33,24}$ . Mestinon® works by inhibiting AChE and thus increasing the amount or potential of ACh to interact with available receptors<sup>24,33</sup>. Additional treatment options, such as immunosuppressive medications or thymectomy, are also available for the clinical management of  $MG<sup>33</sup>$ .

#### **1 .0.4 Electromyographic Assessment of Neuromuscular Transmission**

#### *Repetitive Nerve Stimulation*

Repetitive nerve stimulation (RNS) is <sup>a</sup> putative electrodiagnostic test for confirming disorders of NMT such as  $MG^{5,7,23,33}$ . The theoretical foundation of RNS relies on physiological principles of signal transmission across the  $NMJ<sup>19,32,21</sup>$ . In 1941, Harvey and Masland first noted experiments involving repetitively stimulating <sup>a</sup> nerve supramaximally and recording the compound muscle action potential (CMAP) over the appropriate muscle end-plate as a method to test for NMT disorders $12,26$ . The CMAP, the

primary outcome measure for RNS, represents the summation of all the MFAPs in <sup>a</sup> muscle following supramaximal stimulation of the appropriate motor nerve<sup>5,10</sup>. Although RNS is a straightforward technique, researchers have elucidated important considerations and assumptions that must be understood when using it as an investigational tool. Nervemuscle selection, limb temperature, recording techniques and stimulation parameters are specific components of RNS that have undergone critical review  $5.7,12$ .

<sup>A</sup> standard low frequency RNS protocol employs <sup>a</sup> train of 4-10 supramaximal stimuli applied to a nerve at frequencies between 2-3  $\text{Hz}^{10,31,43}$ . Stimulation frequencies must be kept low enough to prevent calcium  $(Ca^{2+})$  accumulation<sup>5</sup>. Surface electrodes are positioned over the appropriate muscle of interest to record the resultant  $\text{CMAP}^{26,5,12,10}$ . During RNS, immediately releasable ACh quanta stores are progressively depleted $^{23,5,7,26}$ . After the  $4<sup>th</sup>$  stimulation of the RNS protocol, with less ACh available to interact with AChRs, an observable reduction in the EPP is evident<sup>5,7,26</sup>. However, in healthy subjects the reduction in EPP remains above threshold values and is able to generate a  $MFAP^{23,5,7}$ . After 1-2 seconds, secondary ACh stores are mobilized to match the discharge rate resulting in a subsequent recovery of EPP towards the end of the RNS train<sup>5,7,26</sup>. Therefore, in healthy subjects, the negative peak CMAP amplitude remains constant with RNS23,5,7,1°.

However, if enough muscle fibers experience NMT failure, such as in MG, the resultant negative peak CMAP amplitude is reduced<sup>33,23</sup>. The RNS results of a patient with MG are characterized by <sup>a</sup> stereotypical U-shaped response pattern of the CMAP negative peak amplitude<sup>33,26</sup> (Figure 1.2). The initial CMAP response is of normal amplitude and the  $2<sup>nd</sup>$  to  $4<sup>th</sup>$  responses show a progressive decrement of amplitude representing NMT failure at hundreds of muscle fibers<sup>23</sup>. As the immediate releasable ACh quanta stores become depleted, in contrast to their healthy counterparts, an increasing number of EPPs in patients with MG become sub-threshold and thus unable to transmit MFAPs<sup>5,7,26</sup>. As the mobilization stores of ACh quanta are activated, a subsequent improvement in CMAP amplitude may result but these values typically do not return to normal without <sup>a</sup> period of rest. Decrement is calculated by comparing the lowest negative peak CMAP amplitude with the initial response from the RNS train<sup>5</sup>. Decrement of  $\geq 10\%$  change from the CMAP amplitude of the normal response are typically used as the cut-off value for an abnormal result in patients with  $MG^{33,23,10}$ . This inability to generate MFAPs with RNS correlates with symptoms of weakness and fatigue in this patient population.

The low-frequency stimulations (2-3 Hz) used in standard RNS protocols are not representative of true physiological firing rates of motor nerves which during maximal voluntary contractions may reach or exceed 30  $Hz<sup>21,5</sup>$ . This is important because the number of quanta released upon motor nerve stimulation depends both on the number available for immediate release as well as the probability of release<sup>5</sup>. Increased or prolonged  $Ca^{2+}$  influx into the motor axon terminal, evident with higher stimulation frequencies, improves the probability of releasing ACh quanta<sup>5,7,12</sup>. This phenomenon is referred to as  $Ca^{2+}$  facilitation<sup>12,5,7</sup>. Rapid RNS, at stimulation frequencies of 10-50 Hz, can be used to demonstrate  $Ca^{2+}$  facilitation<sup>12,5,7</sup>. However, high stimulation frequency RNS can cause discomfort and pain for the subject and is often not well-tolerated. To improve diagnostic yield, integrating maximum voluntary exercise into a standard low

frequency RNS protocol has been substituted as <sup>a</sup> less painful alternative for high frequency  $RNS^{5,31}$ .

When adding exercise to <sup>a</sup> standard slow RNS protocol, the subject is asked to exercise the muscle by performing an isometric contraction, for  $5{\text -}10 \text{ s}^{7,26}$ , followed immediately by a RNS train to examine for repair of any decrement<sup>5</sup>. More recently, investigators have also employed <sup>a</sup> longer exercise period of up to <sup>1</sup> min in addition to examining RNS after the initial brief period of exercise<sup>43,5</sup>. Immediately after cessation of the 1 min exercise period, slow RNS trains at  $30 s - 1$  min intervals are applied for a period of approximately 5 minutes<sup>11</sup>. Healthy individuals may demonstrate a brief increase in negative peak CMAP amplitude, termed pseudo-facilitation<sup>30,31,12</sup>, following this protocol. Although there is no increase in the number of MFAPs contributing to the CMAP, exercise may cause the MFAPs to fire more synchronously<sup>26,21,7</sup>. Summation of the MFAP responses will produce an increase in CMAP amplitude, <sup>a</sup> slight decrease in CMAP duration, with little change in overall CMAP area<sup>5,30</sup>.

Patients with MG demonstrate an improvement in the CMAP decrement demonstrated during resting RNS at the 3 s and 15 s time intervals post-exercise<sup>7</sup> of either the brief or <sup>1</sup> min exercise periods. The initial improvement in CMAP amplitude, referred to as post-activation facilitation (Figure 1.2), can be explained by the temporary increase in the number of ACh quanta available for release due to improved  $Ca^{2+}$ concentration<sup>26,7,31,23</sup>. At 3-4 minutes post-exercise, initial repair of CMAP is absent and decrement may worsen compared with values obtained during resting RNS, <sup>a</sup> phenomenon termed post-activation exhaustion<sup>26,7,31,23</sup>(Figure 1.2). The exact mechanism for post-exercise exhaustion remains controversial, however researchers have proposed receptor desensitization and <sup>a</sup> reduction in the availability of ACh vesicles as potential candidates mediating this response<sup>7,23,37</sup>. Overall, RNS protocols encompassing an exercise regime currently provide an important diagnostic tool and surrogate measure of fatigue in patients with MG.

#### *Single Fiber Electromyography*

In 1964, Professor Erik Stalberg introduced single-fiber electromyography (SFEMG) as an electrodiagnostic test for disorders of  $NMT<sup>8,10</sup>$ . In SFEMG, a concentric needle electrode is inserted into the muscle end-plate region to obtain extracellular recordings of single muscle fiber action potentials  $(MFAPs)^{7,8}$ . The needle position is adjusted to achieve responses, with sufficient amplitudes and sharp rise times, from a pair of muscle fibers within the same  $MU<sup>11</sup>$ . The MN can be activated either by electrical stimulation or by voluntary contraction<sup>7</sup>. When a MN is repeatedly activated, a natural variability in NMT time across the corresponding individual NMJs is evident due to fluctuating thresholds required to trigger a MFAP post-synaptically<sup>8</sup>. This variability in transmission is termed jitter<sup>23,33</sup>. Normal ranges of jitter values differ between muscle groups<sup>7</sup> and jitter is increased in  $MG<sup>16,10</sup>$ . In pathological conditions, blocking may also occur where an individual muscle fiber within a pair fails to fire altogether<sup>7</sup>. SFEMG is a reliable technique to detect pathologically increased jitter and blocking in disorders of  $NMT^{6,8,23}$ .

#### *Specificity and Sensitivity*

When considering the advantages and disadvantages of various diagnostic tests available for use in MG, it is valuable to examine the relative specificities and sensitivities of each measure. The sensitivity of a technique represents the probability of







Figure 1.2. Repetitive Nerve Stimulation. Panel <sup>1</sup> (left) represents axillary to deltoid stimulation. Panel <sup>2</sup> (right) represents spinal accessory to trapezius stimulation. Results from a representative control subject and a subject with MG are shown using a scale of <sup>2</sup> mV by <sup>2</sup> ms per <sup>a</sup> division. An approximate percent decrement of CMAP amplitude for each stimulation train is indicated in the figure. Post-activation facilitation trains were applied immediately following <sup>10</sup> <sup>s</sup> of exercise. Post-activation exhaustion trains were applied <sup>3</sup> min after 1 min of exercise.

correctly detecting the presence of a given abnormality<sup>8</sup>. In comparison, the specificity of <sup>a</sup> technique indicates the likelihood of correctly identifying the absence of <sup>a</sup> given abnormality<sup>8</sup>. Decreasing the potential for a false negative result will increase the sensitivity, whereas decreasing the potential for <sup>a</sup> false positive result will improve the specificity of a given measure<sup>8</sup>. As it is not possible for a technique to exist with a high probability of detecting both the presence and absence of a given abnormality, sensitivity and specificity share an inverse relationship.

Electrodiagnostic evaluations, such as RNS and SFEMG, are sensitive to NMT failure<sup>38</sup>. Although decrement upon RNS is sensitive for indicating impaired NMT, it is not specific for  $MG<sup>23</sup>$ . The sensitivity of RNS in MG is enhanced by testing multiple symptomatic proximal muscles where the skin temperature at the recording site has been warmed to approximately  $35^{\circ}C^{10,11}$ . Even when these considerations are met, only 75-95% of patients with MG have positive  $RNS<sup>23,10,35</sup>$ . Although time-consuming and technically challenging, the improved resolution obtained with SFEMG yields <sup>a</sup> higher sensitivity  $(90-99\%)^{35}$  for detecting NMT abnormalities in comparison with RNS<sup>33,23</sup>. However, in both techniques the likelihood of detecting false positive results from other neurogenic or myogenic disorders makes improving the specificity of electrodiagnostic testing for MG difficult<sup>33,8</sup>. Other diagnostic measures, such as serologic testing for anti-AChR antibodies, have high specificity for  $MG<sup>33</sup>$ . Auto-antibodies are detectable in approximately 70-90% of cases of  $MG^{39,35,18,7}$ . Integrating additional evaluations of fatigue and weakness may aid in alleviating the limitations of RNS, SFEMG, and serologic testing in developing a comprehensive understanding of MG.

#### **1 .0.4 Neuromuscular Fatigue and Weakness in Myasthenia Gravis**

The well established etiology of fatigue in MG creates the opportunity to apply contemporary research techniques to further our understanding of the functional implications of the disease. Neuromuscular fatigue, hereafter referred to as fatigue; and muscle weakness are interrelated but distinct occurrences. Fatigue is described as <sup>a</sup> deficit in a muscle's ability to sustain a given or required force over time<sup>15,5,14</sup>. In comparison, muscle weakness is defined by <sup>a</sup> loss of strength within <sup>a</sup> given muscle independent of previous physical work or activity<sup>15</sup>. Both a subjective evaluation and force measurement are useful for a comprehensive analysis of fatigue and weakness $27,14$ .

<sup>A</sup> subjective evaluation of fatigue is accomplished through the use of questionnaires and surveys<sup>27,17,36</sup>. The Myasthenia Gravis Fatigue Scale (MGFS)<sup>27</sup> represents one of the few disease-specific fatigue questionnaires available for use in MG. Using <sup>a</sup> Likert-scale format, the MGFS attempts to quantify the subjective experience of fatigue by including <sup>23</sup> items addressing the constructs of depression, disease severity, as well as cognitive and physical fatigue. In addition, visual analogue scales (VAS) are employed as <sup>a</sup> complementary method of evaluating subjective perceptions of fatigue in this population.

Strength measurements are important for disease management in MG. Manual muscle testing  $(MMT)^{2,42,34}$  is a standard technique used clinically to assess muscular strength. Each muscle tested is graded from <sup>0</sup> to 5, with 0 representing no contraction and 5 indicating normal power<sup>13</sup>. Scores of 4 signify active movement against gravity and resistance and can be further subdivided to 4-, 4, 4+ to correlate with slight, moderate, and strong applied resistance, respectively<sup>13,1</sup>. The Quantitative Myasthenia Gravis Score  $(OMG)<sup>4</sup>$ , an instrument used to test the strength of 13 different muscle groups has also been validated as <sup>a</sup> useful investigational tool when assessing weakness and disease severity. Both MMT and the QMG, although requiring specially trained personnel for administration, are efficient and cost-effective ways of assessing muscle strength.

In most cases, results from <sup>a</sup> subjective analysis of fatigue are consistent with traditional physical strength measurements. As previously described, decrement upon RNS correlates with fatigue and weakness experienced in this population. However, <sup>a</sup> subset of patients with MG paradoxically express symptoms of weakness and fatigue in affected muscle groups without demonstrating decrement with RNS studies performed on the same muscle groups. Thus, more information is required to illuminate potential justifications for this apparent discrepancy in the fatiguing characteristics of patients with and without decrement upon RNS.

Although useful measures exist to evaluate muscle strength in MG, quantifying fatigue requires directly measuring force production through the use of a dynamometer<sup>9</sup>. Clinically weak muscles work at <sup>a</sup> higher percentage of their maximal capacity while performing everyday tasks and thus may also exhibit unique fatiguing characteristics<sup>15</sup>. Despite presenting as <sup>a</sup> prototypic fatiguing disorder, limited research has been invested into quantifying fatigue in MG.

Selection of appropriate muscle groups, contraction protocols and intensities are important parameters to consider when designing a fatigue protocol<sup>9</sup>. Protocols involving maximal effort voluntary isometric contractions (MVIC) have been reliably applied to studies examining fatigue in patients with multiple sclerosis  $(MS)^{44,40}$ . Isometric contractions are defined by the production of increasing tension with a constant muscle length. Measuring time to task failure or percentage drop of initial force within a predetermined time are two fatigue indexes which have been used to facilitate group comparison in studies involving patient population groups<sup>29,44</sup> and the elderly<sup>3,22</sup>. Applying <sup>a</sup> fatigue protocol incorporating changes in force as the primary outcome measure provides <sup>a</sup> logical approach to objectively compare fatigue and weakness in patients with MG who present with varying RNS results. Quantitative indicators of fatigue and weakness may provide indirect evidence of NMT failure in patients who do not show decrement with RNS. Alternatively, objective measurement of fatigue might show a pattern of differentiating NMT failure from non-NMT failure causes for weakness and fatigue. In addition, the adequacy of RNS as <sup>a</sup> surrogate measure of fatigue may be further validated.

The objective of this thesis was to evaluate the strength and fatigue of patients with MG who present with and without decrement and to further determine whether the pattern of weakness in MG patients with normal RNS differs from those with decrement and controls.

#### *Objectives*

- 1. To compare shoulder abduction maximum isometric strength in patients with MG in comparison to controls.
- 2. To compare the strength and fatigue of patients with MG who show decrement with RNS to patients who do not show decrement with RNS and control subjects.
- 3. To compare the recovery phase following a fatigue protocol of patients who show decrement with RNS with patients who do not show decrement with RNS and control subjects.
- 4. To measure the subjective perception of fatigue in patients with MG and control subjects with the Myasthenia Gravis Fatigue Survey (MGFS) and <sup>a</sup> brief visual analogue scale.
- 5. To measure the strength and disease severity of patients with MG with traditional manual muscle testing and the Quantitative Myasthenia Gravis Score.

#### *Hypotheses*

- 1. Patients with MG who show decrement with RNS will have reduced strength <sup>i</sup><sup>n</sup> comparison to patients who do not show decrement and to control subjects.
- 2. Patients with MG who do not have decrement with RNS will demonstrate strength similar to control subjects.
- 3. The fatigue index of patients who show decrement upon RNS will be greater than patients who do not show decrement with RNS and control subjects.
- 4. There will be no difference between the fatigue index of patients who do not show decrement with RNS and control subjects.
- 5. Patients who do not show decrementing upon RNS, and control subjects will recover their initial strength before patients who show decrement upon RNS.
- 6. Control subjects will have lower subjective ratings of fatigue compared to patients with MG.
- 7. There will be no difference in the subjective fatigue rating of patients who show decrement with RNS and patients who do not show decrement with RNS.

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#### **CHAPTER 2**

# **QUANTITATIVE ASSESSMENT OF STRENGTH AND FATIGUE IN PATIENTS WITH MYASTHENIA GRAVIS**

#### **2.0 INTRODUCTION**

Patients with myasthenia gravis (MG) characteristically present with fatigable muscle weakness resulting from impaired neuromuscular transmission  $(NMT)^{24,25,36}$ . NMT failure is demonstrated electrophysiologically by decrement of the compound muscle action potential (CMAP) amplitude in response to repetitive nerve stimulation  $(RNS)^{6,8,24}$ . A decrement of  $\geq 10\%$  of the CMAP amplitude when comparing the initial response to the fourth response with low frequency repetitive stimulation is typically considered abnormal in this population  $8.9,12.36$ . Although decrement upon RNS is sensitive for detecting impaired NMT, it is not specific for  $MG<sup>24,12,30</sup>$ . Additional diagnostic measures, such as serologic testing for anti-acetylcholine receptor (AChR) antibodies, have high specificity for  $MG<sup>21,36</sup>$ . Paradoxically, a subset of seropositive patients with MG fails to show decrement upon RNS despite symptoms of weakness and fatigue.

Quantifying <sup>a</sup> decline in force over time is another putative approach used to investigate muscle fatigue<sup>10,28,47,46</sup>. However, despite presenting as a prototypic fatiguing disorder, few studies have directly measured force to evaluate weakness or fatigue in myasthenia<sup>19,26</sup>. The use of questionnaires<sup>27,39</sup> and surveys<sup>49,45</sup>, in addition to manual muscle testing  $(MMT)^{1,13}$ , have emerged as preferred tools to assess weakness and fatigue clinically in MG.

Studies of patients with other neuromuscular disorders (NMD) have applied integrative approaches which incorporate direct force measurements. Schillings et al.<sup>46</sup> reported that patients with NMD experienced <sup>a</sup> higher level of fatigue but lower peripheral fatigue than controls as determined by self-report questionnaires and a twominute sustained maximal voluntary contraction (MVC) of the biceps brachii. Investigators attributed the lower peripheral fatigue observed in NMD to their ability to better maintain the intracellular environment of the muscle due to <sup>a</sup> lower intramuscular pressure produced by smaller MVCs. A study by Garssen et al.<sup>17</sup> examining the residual fatigue of patients with Guillain-Barré syndrome (GBS) supported the aforementioned findings of <sup>a</sup> higher level of experienced fatigue in the patients versus controls. In addition, for the first minute of <sup>a</sup> two-minute sustained MVC of the biceps brachii, patients with GBS developed peripheral fatigue more slowly than controls which aligns with results from patients with other NMD. Overall, the multidisciplinary methodology used to study weakness and fatigue in other NMD provides <sup>a</sup> viable framework to study weakness and fatigue using a myasthenic model.

The aim of the present study was to objectively measure strength and fatigue in <sup>a</sup> cohort of patients with MG who present with varying RNS results. We hypothesized that quantitative indicators of weakness and fatigue may provide indirect evidence of NMT failure in patients who do not show decrement with RNS. Additionally, objective measurement of fatigue might show a pattern differentiating NMT failure from non-NMT failure causes for weakness and fatigue in myasthenia. Lastly, the adequacy of RNS as <sup>a</sup> surrogate measure of fatigue may be further validated.

#### **2.1 METHODS**

#### **2.1.1 Subjects**

Twenty patients with clinical features of generalized MG, followed through the MG clinic at London Health Sciences Center, were invited to participate in the study. Patients were included if they were seropositive for acetylcholine receptor (AChR) antibodies and indicated self-reported symptoms of weakness or fatigue of their shoulder girdle muscles. In addition, <sup>a</sup> group of <sup>21</sup> healthy control subjects without evidence of neuromuscular or musculoskeletal disorders volunteered to participate. Any individuals presenting with other conditions that could cause weakness or fatigue were excluded from the study. All subjects provided informed written consent and the study was approved by The University of Western Ontario, Health Sciences Research Ethics Board.

#### **2.1.2 Fatigue Questionnaires**

All data were collected during <sup>a</sup> single visit to the Neuromuscular Assessment Laboratory at University Hospital (London, Ontario). At the beginning of the study visit, all participants completed the MG Fatigue Survey  $(MGFS)^{27}$  (Appendix A) and a 2-item visual analogue scale (VAS) (Appendix B). The MGFS is <sup>a</sup> Likert scale containing <sup>26</sup> items addressing <sup>3</sup> sub-scales of fatigue including perception of fatigue, task avoidance behaviors, and observable motor signs associated with fatigue<sup>27</sup>. Potential scores range from 25 to 130, with higher scores indicating greater fatigue<sup>27</sup>. For each item of the VAS, subjects were instructed to quantify their responses by intersecting <sup>a</sup> <sup>10</sup> centimeter horizontal line anchored with various descriptors at either end. The 2-items of the VAS specifically asked subjects to quantify their current level of fatigue and respond to how their fatigue has impacted their activities of daily living (ADL) within the past month.
Both measures, MGFS and VAS, were included to provide subjects with the opportunity to assess their individual fatigue characteristics.

#### **2.1.3 Clinical Examination**

The disease severity of patients with MG was evaluated by an experienced advanced practice nurse using the modified Quantitative MG Score for Disease Severity Assessment (13 muscles tested)  $(OMG)^5$  (Appendix C) and the MG Activities of Daily Living Scale (MG-ADL)<sup>49</sup> (Appendix D). The QMG is a Likert scale with a potential score range of <sup>0</sup> to 39, with higher scores indicating greater muscle weakness and disease severity<sup>5</sup>. The grade assigned to each muscle tested by the QMG ranges from 0 to 3, where  $0 =$  no muscle weakness and  $3 =$  severe muscle weakness. The OMG score associated with shoulder muscle weakness was evaluated independently within the groups. The MG-ADL is also <sup>a</sup> Likert scale, with potential scores ranging from <sup>0</sup> to 24, with higher scores suggesting greater disease severity<sup>49</sup>.

In addition, <sup>a</sup> neurologist (Dr. M. W. Nicolle, director of MG Clinic, London Health Sciences Centre) evaluated the strength of 7 upper extremity muscle groups (neck flexors, neck extensors, deltoid, biceps, triceps, wrist flexion, and wrist extension) of each patient using the Medical Research Council (MRC) Scale<sup>13</sup> for manual muscle testing (MMT)<sup>37,15</sup>. Baseline and fatigue MMT strength measurements were determined testing (MMT)<sup>37,15</sup>. Baseline and fatigue MMT strength measurements were determined<br>for each muscle group. Raw scores for each muscle group from the MMT were converted to a 10 point scale<sup>15</sup> and summed to determine an overall Megascore ranging from  $0-70$  points<sup>15</sup>. The converted deltoid muscle baseline and fatigue MMT scores were compared within each patient group.

#### **2.1.4 Spinal Accessory and Axillary Nerve Repetitive Nerve Stimulation**

Proximal nerve-muscle combinations are more commonly and typically more severely affected in patients with MG in comparison to more distal muscles<sup>41</sup>. Thus, repetitive stimulation of the spinal accessory nerve to trapezius and the axillary nerve to deltoid were performed on the dominant side of all participants. Patients withheld taking anticholinesterase medications (e.g. ®Mestinon) for at least <sup>5</sup> h prior to their study visit. For each nerve studied, subjects were in <sup>a</sup> supine position with their arm at their side. Limb muscles under investigation were warmed with the aid of <sup>a</sup> heat lamp. After preparing the skin with 70% v/v isopropyl alcohol, disposable surface recording electrodes (Ag-AgCl Mactrode Electrodes; GE Medical Systems, Milwaukee, Wisconsin), cut into <sup>10</sup> mm by <sup>30</sup> mm strips, were secured with tape to the appropriate recording sites for the muscle being studied. The spinal accessory nerve was stimulated at the posterior border of the sternocleidomastoid muscle. The active electrode was positioned over the motor point of the trapezius muscle, with the reference electrode positioned over the acromion. The axillary nerve was stimulated at Erb'<sup>s</sup> point, with the active electrode positioned over the motor point of the middle deltoid and the reference electrode was positioned distally over the lateral epicondyle of the humerus. A full sized 27 mm by 22 mm electrode was used as a ground. Electrodiagnostic set-up and technique were consistent with parameters previously described by Preston and Shapiro  $(2005)^{41}$ .

Single cutaneous electrical stimulations of each nerve began at very low stimulation intensities and were gradually increased until the maximal compound muscle action potential (CMAP) amplitude response was obtained. The stimulation intensity was increased an additional 15-20 % to ensure a supramaximal stimulation was delivered during the entire RNS protocol. All studies were completed on <sup>a</sup> standard EMG machine (Advantage Medical, London, Ontario, Canada).

The RNS protocol was identical for both nerves being studied. <sup>A</sup> total of three trains of 10 stimulations, with intensities of  $5 - 60$  mA, were administered at a frequency of <sup>3</sup> Hz with 0.1 - 0.2 ms square pulse durations. The first train was applied with the subject at rest. Post-exercise facilitation was examined by applying <sup>a</sup> second train immediately following <sup>10</sup> <sup>s</sup> of <sup>a</sup> maximal voluntary isometric contraction (MVIC). <sup>A</sup> final train, to examine post exercise exhaustion, was administered <sup>3</sup> minutes after <sup>1</sup> minute of intermittent MVICs. The intermittent exercise for both muscles involved performing <sup>12</sup> cycles of <sup>4</sup> <sup>s</sup> on, <sup>1</sup> <sup>s</sup> off repeats. Auditory feedback and strong verbal encouragement were provided during the MVICs.

Negative peak amplitude (mV), negative peak area (mV∙ms), and the % change of both amplitude and area in comparing the compound muscle action potential evoked by the first and the fourth stimulation of each train were determined. <sup>A</sup> negative % change (decrement) of CMAP amplitude greater than 10% during any train of the RNS protocol of either nerve-muscle combination was considered indicative of significant decrement<sup>36,24,8</sup>. Subjects were divided into three groups (controls, decrementing MG (D-MG), non-decrementing MG (ND-MG)) according to the results of RNS of the spinal accessory and axillary nerves.

#### **2.1.5 Force Measurement**

*Experimental Set-up.* <sup>A</sup> Biodex System <sup>3</sup> dynamometer (Biodex Medical Systems, Shirley, New York) was used to assess the shoulder abduction torque of the dominant side of all participants. Subjects were seated in the adjustable Biodex chair facing away from the dynamometer with <sup>a</sup> seat rotation of 90° and <sup>a</sup> hip joint angle of 85°. Two diagonal shoulder straps and <sup>a</sup> waist strap were used to stabilize the subject'<sup>s</sup> position in the chair. The dynamometer, with a tilt of 10°, was adjusted so that the axis of rotation of the shoulder (glenohumeral joint) aligned with the axis of rotation of the dynamometer arm. The subject'<sup>s</sup> dominant arm, with 90° of elbow flexion, was secured with wide Velcro straps in <sup>a</sup> custom-made attachment positioned over the deltoid tuberosity.

The isometric exercise mode for 30° of shoulder abduction was selected using the Biodex Advantage software (version 3.14). The raw isometric shoulder abduction force, obtained from the Biodex, was converted from analog to digital format by <sup>a</sup> 12-bit converter (CED model <sup>1401</sup> Plus, Cambridge Electronic Design, Cambridge, UK) with <sup>a</sup> torque scaling of <sup>347</sup> N∙m and <sup>a</sup> sampling rate of <sup>100</sup> Hz. Torque production, measured in N∙m, was displayed visually to the subject, in real-time, on <sup>a</sup> computer screen using Spike <sup>2</sup> software (Spike 2, version 5.14; Cambridge Electronic Design, Cambridge, United Kingdom).

*Experimental Protocol.* The experimental contraction protocol consisted of three phases of force measurement: baseline, fatigue, recovery (Figure 2.1). Following an explanation of the proper contraction technique, subjects completed <sup>a</sup> warm-up of <sup>15</sup> submaximal isometric shoulder abduction contractions consisting of <sup>3</sup> <sup>s</sup> on, <sup>1</sup> <sup>s</sup> off repeats. Visual feedback and strong verbal encouragement were provided during all contractions. After the warm-up, subjects were instructed to perform 3, <sup>3</sup> <sup>s</sup> MVICs separated by <sup>a</sup> <sup>2</sup> min rest period. Maximal voluntary muscle tension has been shown to have a definite and repeatable value compared with tetanic stimulation<sup>34</sup>. For each

subject, the MVIC with the largest peak torque value was selected for subsequent comparison against fatigue and recovery contractions. <sup>A</sup> target line, normalized to the subject'<sup>s</sup> highest peak torque produced during the baseline contractions, was drawn on the computer screen. Subjects were instructed to use the target line for guidance to continue to exert <sup>a</sup> maximal effort during each of the remaining contractions. Fifteen minutes of rest were provided following the baseline measurements. In order to determine fatigue, the subjects then performed <sup>a</sup> series of <sup>12</sup> intermittent MVICs consisting of <sup>4</sup> <sup>s</sup> on, <sup>1</sup> <sup>s</sup> off repeats. Fatigue was calculated by recording and comparing changes in peak torque (N∙m) values across all contractions. The recovery phase consisted of single <sup>3</sup> <sup>s</sup> MVICs at 0.5, 1, 3, 5, 10, and <sup>15</sup> minutes following cessation of the fatiguing phase of contractions. All MVICs during the fatigue protocol were analyzed offline, using Spike 2 software, for peak torque values.

#### **2.1.6 Statistical Methods**

Mean values and standard deviations (SD) are presented for all parameters. Group variances were not equal, thus primarily non-parametric statistics were used to analyze the data. To compare the subjective perception of fatigue in patients with MG and control subjects, results from the MGFS and VAS were analyzed using <sup>a</sup> Kruskal-Wallis test followed by Dunn'<sup>s</sup> Multiple Comparison post-hoc test to determine individual group differences. <sup>A</sup> Mann-Whitney test was used to compare disease severity between D-MG and ND-MG patient groups for both the QMG and MG-ADL scales. Baseline and fatigue MMT strength measurements for the deltoid muscle were compared separately for D-MG and ND-MG patient groups using a two-tailed paired t-test.

Normalized initial MVIC peak torque values were compared across groups using <sup>a</sup> Kruskal-Wallis test. Within each group, change in peak torque over time was analyzed using <sup>a</sup> repeated measures ANOVA across all <sup>12</sup> contractions. Peak torque values normalized to individual MVICs of contraction numbers 1, 6, and <sup>12</sup> of the fatigue protocol were further compared between groups using <sup>a</sup> Kruskal-Wallis test. <sup>A</sup> Bonferonni correction, with an  $\alpha$  level set at 0.017, was applied to determine individual group differences. <sup>A</sup> repeated measures ANOVA, with <sup>a</sup> square root transformation to improve equality of variance, was used to compare the recovery peak torque values between groups. An analysis of covariance, adjusting for MVIC, was used to compare the 0.5 and <sup>15</sup> minute recovery contractions between groups.

Data were analyzed using GraphPad Prism version 4.00 for Windows (GraphPad software, San Diego, California).

#### **2.2 RESULTS**

#### **2.2.1 Subject Characteristics**

Subject characteristics are presented in Table 2.1. Participants ranged in age from 22 to 81 years, with an average age of 53.61 years ( $SD = 18.37$  years). The majority of subjects were of Caucasian descent, with the exception of one Egyptian subject belonging to the D-MG group. According to international classification standards for body mass index (height (m) / weight  $(kg)^2$ ), on average both patient groups were overweight (BMI  $\geq$  25.00) whereas control subjects were within normal ranges (BMI, 18.50 – 24.99).



Figure 2.1. Example of experimental protocol. Data is representative of <sup>a</sup> male control subject. The x-axis, time (min), is not drawn to scale. See text for details. (MVIC = maximal voluntary isometric contraction).

The majority of patients were currently taking AChE medications, such as ®Mestinon, as a part of their symptomatic treatment regime.

#### **2.2.2 Fatigue Questionnaires and Clinical Examination**

An overview of scores resulting from the MGFS, QMG, and MG-ADL clinical instruments are included in Table 2.2. According to the MGFS, ND-MG patients experience more fatigue compared with control subjects ( $p < 0.05$ ). The D-MG patients also describe greater fatigue than control subjects ( $p < 0.001$ ). However, the fatigue scores between patient groups were not different. Results from the 2-item VAS were consistent with the MGFS scores. When subjects were asked to quantify their current level of fatigue, D-MG patients indicated a higher level of fatigue compared with control subjects ( $p < 0.01$ ). In the past month relative to testing, fatigue also had a greater impact on ADL in the ND-MG and D-MG groups compared with controls ( $p < 0.01$  and  $p < 0.001$ , respectively). In summary, subjective appraisal of the degree of fatigue experienced between ND-MG and D-MG groups appears similar and both patient groups describe greater fatigue compared with controls.

The clinical evaluation of patients with MG, using the QMG and MG-ADL scales in addition to MMT, yielded valuable information concerning the disease severity and muscle strength differences between groups. According to the QMG score, the D-MG group had a greater disease severity compared with the ND-MG group ( $p < 0.05$ ). When examining the QMG score for shoulder weakness independently, the D-MG group demonstrated mild shoulder weakness  $(1.25 \pm 0.86, \text{mean} \pm \text{SD})$  whereas the ND-MG group did not demonstrate any shoulder weakness  $(0.33 \pm 0.50, \text{mean} \pm \text{SD})$ . The scores on the MG-ADL scale provided consistent results, indicating that the D-MG group experienced more severe fatigue compared with the ND-MG group ( $p < 0.01$ ). All of the patients within the ND-MG group had normal strength at the baseline MMT assessment of each of the included muscle groups. In comparison, the D-MG group achieved <sup>a</sup> mean overall MMT Megascore of 67.53 (SD = 2.43), with scores ranging from 61 to 70. The deltoid muscle of both patient groups had reduced strength at the fatigue MMT assessment compared with baseline MMT scores (D-MG group, <sup>p</sup> <sup>&</sup>lt; 0.0001; ND-MG group,  $p < 0.05$ ). In summary, a clinical evaluation of both patient groups indicated that the D-MG group had greater disease severity, but similar baseline upper extremity strength as the ND-MG group.

## **2.2.3 Repetitive Nerve Stimulation**

<sup>A</sup> summary of the percent decrement values of the recorded CMAP response upon RNS are included for both spinal accessory and axillary nerve stimulations in Table 2.3 and Table 2.4, respectively. Values indicate <sup>a</sup> comparison of negative peak amplitude (NpAmp) between the first and the fourth CMAP response<sup>8</sup>.

#### **2.2.4 Force Measurement**

Peak torque (N∙m) and peak torque normalized to MVIC torque values for the shoulder abduction fatigue test contractions are displayed in Figure 2.2. Controls had greater MVIC force compared with the patient groups ( $p \le 0.001$ ). Further, the ND-MG group had greater MVIC force compared with the D-MG group. Within all three groups force decreased with time  $(p < 0.001)$ . Between groups analysis revealed that peak torque values normalized to MVIC were different between controls and the D-MG group at contraction #6 ( $p = 0.016$ ). No between group differences were found at contraction #1





 $\alpha$ 

 $\mathcal{L}^{\text{max}}_{\text{max}}$  and  $\mathcal{L}^{\text{max}}_{\text{max}}$ 

BMI= body mass index, AChE <sup>=</sup> acetylcholinesterase

# Table 2.2. Clinical Scales



MGFS <sup>=</sup> myasthenia gravis fatigue survey, QMG <sup>=</sup> quantitative myasthenia gravis score, MG-ADL = myasthenia gravis activities of daily living scale



Table 2.3. Repetitive Nerve Stimulation of Spinal Accessory Nerve

ND-MG <sup>=</sup> non-decrementing myasthenia gravis, D-MG <sup>=</sup> decrementing myasthenia gravis, NpAmp <sup>=</sup> negative peak amplitude, CMAP <sup>=</sup> compound muscle action potential,  $n =$  number of subjects



## Table 2.4. Repetitive Nerve Stimulation of Axillary Nerve

ND-MG <sup>=</sup> non-decrementing myasthenia gravis, D-MG <sup>=</sup> decrementing myasthenia gravis, NpAmp <sup>=</sup> negative peak amplitude, CMAP <sup>=</sup> compound muscle action potential,  $n =$  number of subjects

 $\mathcal{L}$ 



Figure 2.2. Fatigue test. A: Peak torque (Nm) values of shoulder abduction fatigue test contractions. B: Peak torque normalized to MVIC torque values for fatigue test contractions. Dashed line indicates one hundred percent of initial MVIC. Data are presented as means  $\pm$  SEM. (MVIC = maximal voluntary isometric contraction).



Figure 2.3. Recovery Phase. A: Recovery phase peak torque (Nm) values for shoulder abduction contractions. B: Peak torque normalized to MVIC torque values for recovery phase contractions. Dashed line indicates one hundred percent of initial MVIC. Data are presented as means  $\pm$  SEM. (MVIC = maximal voluntary isometric contraction).

and  $\#12$  (p > 0.017). Although each group had different initial MVIC force values, the fatigue index between groups was not different.

Recovery phase peak torque (N∙m) and peak torque normalized to MVIC torque values are shown in Figure 2.3. Adjusting for MVIC values, there is no evidence that the behavior during recovery differs between groups ( $p > 0.05$ ). In addition, there is no evidence of <sup>a</sup> difference in recovery between groups at the 0.5 min post-fatigue time  $(p = 0.496)$  and 15 minute recovery times  $(p = 0.823)$ . Overall, there is no difference in recovery between groups.

#### **2.3 DISCUSSION**

The major finding of this study was that fatigue and recovery of normalized peak torque values for shoulder abduction did not differ between patients with MG and healthy controls. However, the baseline maximum voluntary isometric (MVIC) strength differed between groups. The D-MG group produced the lowest MVIC force, followed by the ND-MG group and controls, respectively. All of the ND-MG patients demonstrated normal baseline strength of the upper extremity muscles examined with MMT. The D-MG group exhibited mild weakness according to the overall Megascore obtained from all the upper extremity muscles examined with MMT. Additionally, patients with MG reported experiencing greater fatigue compared with controls. However, self-report fatigue did not differ between D-MG and ND-MG patient groups. Clinical measures, such as the QMG and MG-ADL, indicated that the D-MG group had greater disease severity relative to the ND-MG group.

As weakness and fatigue are predominant characteristics of  $\text{MG}^{20,24,36}$ , the observation that patients with MG report greater fatigue than healthy control subjects is well supported by clinical reports<sup>36,24</sup> and research which has utilized self-report fatigue questionnaires in this population  $40,27,18$ . In the present study, however, higher levels of experienced fatigue in patients with MG did not translate into greater muscle fatigue, as directly measured by <sup>a</sup> force dynamometer, as compared to healthy controls. Similar findings have been reported in studies examining patients with Chronic Fatigue syndrome<sup>48</sup>. Patients with Chronic Fatigue Syndrome complain of weakness and fatigue and experience high levels of effort associated with activity with no apparent differences in measured muscle fatigue compared to healthy controls<sup>48</sup>. In addition, a study examining patients with MS reported no difference in muscle fatigue between patients who reported experiencing high ( $75<sup>th</sup>$  percentile) versus low ( $25<sup>th</sup>$  percentile) fatigue using a multidimensional fatigue assessment tool<sup>42</sup>. In patients with MG, one possible explanation of higher experienced fatigue is that confounding variables, such as physical inactivity, sleep disturbances, and psychological factors, contributed to an increased perception of fatigue. <sup>A</sup> relationship between the pathological decrease in muscle strength and <sup>a</sup> subsequent decrease in physical activity, increase in sleep disturbances, and increase in pain has been determined using other NMD models $^{22,40,18}$ .

The consequence of the maladaptive responses to reduced muscle strength have been further linked to higher levels of experienced fatigue in <sup>a</sup> longitudinal research study using three unique NMD models $^{22}$ . In addition, patients with NMD in the longitudinal research study demonstrated greater central activation failure (CAF) which may indicate reduced motivation or effort related to their higher reported level of experienced fatigue<sup>46</sup>. In a study by Kittiwatanapaisan et al.<sup>27</sup>, a negative correlation between physical activity and fatigue scores was found in patients with MG. The majority of the participants with MG in the Kittiwatanapaisan et al.<sup>27</sup> study were overweight  $(B.M.I \geq 25.00)$  or obese which is a potential side effect of therapeutic steroid medications. The higher B.M.I scores in this group may also be an indirect cause or effect of reduced physical activity, subsequently leading to an increased perception of fatigue. Patients with MG who engage in low-impact exercise have reported lower fatigue severity scores and improved functional capacity compared to their inactive counterparts<sup>18</sup>. In the present study although the physical activity status of patients was not measured, the majority of patients with MG were overweight or obese. The interaction between experienced fatigue and physiological muscle fatigue merits further investigation. In addition, determining the impact of confounding variables such as physical inactivity, sleep disturbances, and psychological variables on experienced fatigue in patients with MG will offer the opportunity to implement new strategies to reduce experienced fatigue in this population.

The D-MG and ND-MG patient groups did not differ in their reported level of experienced fatigue. The origin of experienced fatigue in both patient groups may be related to the same aforementioned confounding factors which have the potential to arise in addition to the fundamental pathophysiology of MG, that is, NMT failure. Alternatively, as the sensitivity of RNS for detecting NMT failure is not as high as other techniques such as  $SFEMG<sup>8,36</sup>$ , RNS results may not accurately reflect experienced fatigue. A study by Rostedt et al. $43$  found no correlation between a global functional fatigue questionnaire score and RNS results of the deltoid muscle in patients with MG.

The global fatigue questionnaire score was derived from individual scores on the myasthenia gravis questionnaire developed by Padua et al.<sup>39</sup> and the short form questionnaire (SF-36). However, <sup>a</sup> positive correlation was found between the global questionnaire score and jitter and blocking on SFEMG results. The increased time and patient co-operation required for SFEMG, made RNS <sup>a</sup> more preferable alternative for differentiating patient groups in the present study.

According to clinical indicators, the D-MG patient group had more severe MG relative to the ND-MG group. Early animal studies have supported a relationship between disease severity and positive RNS results. For example, an experiment by Berman et al.<sup>7</sup> using <sup>a</sup> murine model of experimental autoimmune myasthenia gravis (EAMG) found decrement upon RNS with all moderately affected mice. In comparison, weakly myasthenic mice did not always demonstrate decrement<sup>7</sup>. Rat and guinea pig models with EAMG have also revealed that some animals demonstrate muscle weakness with no electrophysiological correlates<sup>29</sup>. In the current study, both patient groups with MG were weaker in comparison to healthy control subjects. Further, D-MG patients were weaker than ND-MG patients. Upper extremity weakness detected by MMT was found to relate to decrement upon RNS, but was not able to detect the mild weakness found by direct force measurement in the ND-MG group. The greater reduction in muscle strength evident in the D-MG patient group may be explained by the corresponding greater disease severity of the group.

No overall difference in normalized fatigue or recovery force of shoulder abduction MVIC was evident between groups. <sup>A</sup> difference in normalized fatigue was found at contraction #6 between the D-MG group and controls, but that difference was not apparent by contraction #12. Thus, in the first half of the contraction protocol fatigue developed more rapidly in the D-MG group compared to controls.

The absence of <sup>a</sup> difference in recovery between groups is somewhat surprising. Electrophysiological techniques such as RNS which employ exercise have demonstrated that decrement worsens 3-5 minutes post-exercise, a phenomenon referred to as postactivation exhaustion<sup>44,6</sup>. Post-activation exhaustion has been attributed to desensitization of AChR coupled with the reduction of available ACh following exercise<sup>6,8,9</sup>. With worsening decrement, <sup>a</sup> subsequent reduction in the capability of the muscle to recover during the 3-5 minute time epoch following the fatigue test may be expected. Thus, the absence of a difference in recovery between patients with MG and controls has yet to be explained.

Few studies have examined muscle fatigue in proximal muscle groups using <sup>a</sup> myasthenic model. Herbelin et al.<sup>19</sup> used 30 s of maximal effort isometric exercise of hand grip, elbow flexion, elbow extension, knee extension, and ankle dorsiflexion to examine the relationship between isometric fatigue and decrement upon RNS, QMG scores, and MG-ADL scores in MG. Isometric fatigue testing was shown to relate best to decrement upon RNS and was found to account for ten percent of the variability of the QMG and MG-ADL scores. In the present study, as there was no difference in muscle fatigue between D-MG and ND-MG at either 30 <sup>s</sup> time period or at 60 s, fatigue scores of shoulder abduction contractions in MG do not reflect differences in RNS results.

An earlier study by Kimura et al.<sup>26</sup> suggested that MVC contractions may be used to reduce the potential for <sup>a</sup> false negative diagnosis resulting from routine electromyographic assessments in cases of ocular MG. By comparing changes in

parameters, such as EMG pulses and the mean amplitude of the CMAP response, during <sup>a</sup> voluntary MVC protocol, greater muscle fatigue of the orbicularis oculi muscle was found in patients with MG compared to controls. An injection of tensilon, <sup>a</sup> short-acting AChE inhibitor, significantly improved muscle fatigue and recovery in MG compared to controls. However when examining muscle fatigue of proximal limb muscles <sup>i</sup><sup>n</sup> the present study, no difference was found between the fatigability or recovery of patients with MG with varying RNS results and healthy controls subjects. Rest following activity has been shown to relieve fatigue in patients with  $MG^{36,24,25}$ . One possible explanation for the fatigue results in the current study is that adaptations in the muscle distal to the NMJ may occur in patients with MG that favor fatigue resistance with subsequently similar recovery relative to controls.

Shoulder muscle strength of patients with MG was significantly reduced with no difference in muscle fatigue compared to healthy controls. Studies examining fatigue in elderly subjects provide similar findings of preserved endurance accompanying reduced strength<sup>35,3,32,23</sup>. Elderly subjects may experience adaptations in the muscle due to ageing and deconditioning<sup>2,16</sup>. Changes in the fiber composition of the muscle, impairment of high threshold fatigable motor units, and muscle atrophy have all been proposed as potential mechanisms mediating lower muscle fatigue recorded in the elderly<sup>35,3,32</sup>. A decrease in muscle relaxation rate represents another candidate modulating the preservation of force in fatiguing muscles<sup>14,3</sup>. In addition, afferent feedback from peripheral sources during fatigue may impact changes in descending drive from the CNS affecting recruitment and rate coding patterns of  $MNs^{4,14}$ . Although the pathophysiology

of MG is understood as impairment of NMT, the possibility of further adaptations of the muscle or the CNS to accommodate a disturbance in NMT demands further exploration.

A study by McKenzie and Gandevia<sup>33</sup> provides evidence of a relationship between absolute muscle force and fatigability. Subjects performed intermittent MVIC of the elbow flexors or inspiratory muscles at two different muscle lengths, an optimal length and <sup>a</sup> length that is shown to decrease the absolute MVIC by 25%. Although absolute force was different, all contractions were performed with maximal effort relative to each muscle length. Each muscle tested was less fatigued at the shorter length and thus the lower absolute force level. The force-fatigability relationship suggests that the greater the absolute force the more rapidly the muscle fatigues<sup>14</sup>. In patients with MG, the higher anticipated muscle fatigue due to the underlying pathophysiology of the disease may be curtailed by a significantly reduced absolute force compared to controls.

Studies examining other NMD models<sup>46</sup>, including  $GBS<sup>17</sup>$ , have implicated the ability of patients to maintain the integrity of the intracellular state of the muscle due to reduced occlusion of blood flow from lower MVIC torques as <sup>a</sup> potential mechanism to explain reduced fatigue in patients relative to controls. In both studies<sup>46,17</sup>, sustained MVIC contractions were used in comparison to the intermittent MVIC contractions used in the present study. Thus, potential improvement in blood flow in the control subjects with intermittent versus sustained contractions may explain the absence of a difference in fatigue between patients and controls found in the current study. In addition, both Schillings et al.<sup>46</sup> and Garssen et al.<sup>17</sup> found higher central activation failure (CAF) in patients with NMD compared to controls. Higher CAF may account for higher levels of experienced fatigue in these populations<sup>46,17</sup>. Measuring central fatigue, potentially

manifested as higher experienced fatigue, in <sup>a</sup> myasthenia model may provide further insight into physiological adaptations that occur in response to pathological perturbations of the NMJ.

#### **2.4 LIMITATIONS**

It is important to consider the limitations of the present study before attempting to apply the findings to <sup>a</sup> broader population of patients with MG. One limitation of the study was that the sample size of each subject group was small. Approximately 20-25% of patients with MG do not demonstrate decrement upon  $RNS<sup>38</sup>$ . Of that population, finding patients who reported experiencing fatigue of the shoulder made recruitment of the ND-MG group challenging. In addition, <sup>a</sup> large variance existed within and between each group. Efforts were made to achieve <sup>a</sup> similar distribution of both age and gender within groups. However, results from the experimental contraction protocol and the QMG encompassed <sup>a</sup> wide dispersal of values, possibly reflecting the inclusion of both genders and a wide age range of participants within the present study. Particularly within the D-MG group, definite differences in strength were evident. Interestingly, only in some cases did the subjects with greater recorded strength deficits correspond to greater disease severity or level of experienced fatigue in comparison to other group members. Small sample sizes and <sup>a</sup> wide variance within and between each group suggest that results from the present investigation should be applied with caution to the broader myasthenic population.

As only the shoulder muscles were tested, extrapolating the study results broadly to other muscle groups in MG may not be appropriate. Although the shoulder muscles were <sup>a</sup> very reasonable selection given that MG is known to frequently affect proximal limb muscles<sup>36,21</sup>, differences in muscle fatigability which may be attributed to fiber type composition of various muscles $^{31,10}$ , may also differ between affected muscles in MG.

Performing intermittent MVICs of shoulder abduction is not customary in the day to day activities of most individuals. However, MG is <sup>a</sup> peripheral NMJ disorder and in the absence of central fatigue, individuals have been shown to be able to voluntarily maximally activate their deltoid muscle<sup>34</sup>. Central fatigue is not acknowledged as a contributing mechanism of the primary pathological weakness and fatigue in MG. In addition, due to inherent challenges of measuring central fatigue in the given experimental set-up, it was not measured in the present study. In addition, contemporary methods used to measure voluntary drive rely on the assumption that there is no defect in NMT, an assumption which is clearly violated in patients with MG. Although recently, studies have begun to implicate CAF as an important variable to examine when studying weakness and fatigue in other NMD models<sup>46,17</sup>. An increase in CAF in patient populations may act as <sup>a</sup> protective mechanism to prevent any redundant activation of abnormal NMJs. Thus, although muscle fatigue did not differ between patient groups including an indicator of CAF in the present study may have provided valuable information potentially further differentiating patients with MG who present with varying RNS results.

As an electrodiagnostic technique, RNS is also subject to inherent limitations. For example, as previously mentioned, the sensitivity of RNS is not as high as SFEMG. Thus, the potential for false-negative detections of impaired NMT is higher in RNS compared to SFEMG. The sensitivity of RNS was improved in the present study by testing two

symptomatic shoulder girdle muscles and by warming the muscles. In addition, all RNS trials were performed by an experienced EMG technologist. The aforementioned increased patient co-operation and time required to perform SFEMG, made RNS <sup>a</sup> preferred electrodiagnostic technique for differentiating patient groups in the present

symptomatic shoulder girdle muscles and by warming the muscles. In tirals were performed by an experienced EMG technologist. The increased patient co-operation and time required to perform SFEM preferred electrodiagnostic Lastly, fatigue is <sup>a</sup> broad and multidimensional construct. The ability to directly link NMJ failure, as represented by decrement upon RNS, to muscle fatigability in the present study is somewhat limited. Adaptive responses to the underlying NMJ pathophysiology of MG may mask the true impact of NMJ failure on muscle weakness and fatigue in this population. A multidisciplinary approach was used in the present study to limit this problem, however in a clinical population group it is challenging to avoid all potentially confounding variables.

#### **2.5 FUTURE STUDIES**

The present study has succeeded in providing an introductory contribution to research in directly quantifying muscle weakness and fatigue in MG and has thus provided <sup>a</sup> framework to direct future investigations. <sup>A</sup> natural progression from the current findings would be to quantify the fatigue of more muscle groups within <sup>a</sup> myasthenic population. Developing a database of force and torque values for the strength and fatigue of different muscle groups would be useful in future clinical triais with MG. Repeating the present study using SFEMG instead of RNS to detect NMT failure and establishing <sup>a</sup> sub-group analysis based on disease severity, may also yield unique findings.

As experienced fatigue does not correspond to recorded shoulder muscle fatigue, exploring potential confounding variables such as physical inactivity, psychological factors, and sleep disturbances in subsequent investigations is important. Including <sup>a</sup> measurement of experienced fatigue, perhaps by the use of a VAS, at various time points during fatiguing and recovery contractions would provide a more complete understanding of any interactive effects between experienced fatigue and muscle fatigue and recovery within groups. In addition, including an indication of CAF may also shed light on potential differences between patients with MG who present with varying RNS results.

Examining the possibility of physiological adaptations to NMI failure on muscle weakness, fatigue, and recovery represents an alternative arena for future investigations. A plethora of techniques are available to explore the contributions of various elements to muscle fatigue. For example, twitch interpolation is a putative technique used to examine central activation<sup>11,9</sup>. Comparisons between the cross-sectional areas of muscles to examine for muscle atrophy, is possible with magnetic resonance imaging<sup>16</sup>. Biochemical analysis of muscle tissue obtained by <sup>a</sup> needle biopsy may reveal any metabolic adaptations to NMJ failure<sup>16</sup>. The feasibility or necessity of invasive research procedures, such as muscle biopsy, has yet to be determined in this clinical population. The influence of central fatigue in MG provides <sup>a</sup> logical starting point to elucidate other contributing mechanisms to weakness and fatigue following NMT failure.

#### **2.6 CONCLUSION**

The present investigation has achieved the objective of quantifying strength and fatigue in the shoulder muscles of patients with MG who present with varying RNS results. Additional information pertaining to disease severity and experienced fatigue in this population, established from the use of multidisciplinary tools, have aligned with findings from previous investigations. No differences, with the exception of disease severity and muscle weakness, were found between the D-MG and ND-MG group. Differences in RNS results appear to relate most closely with disease severity. Obtaining quantitative measures of weakness, fatigue, and recovery in the muscles of patients with MG have implications in the potential re-evaluation of outcome measures used in clinical triais or in examining the effectiveness of non-pharmacological therapeutic interventions. Future investigations examining different muscle groups, in addition to the contribution of CAF to muscle fatigue, are required. The apparent discrepancy between experienced fatigue and measured muscle fatigue also needs to be resolved. The contributions of the present investigation to the understanding of weakness and fatigue in patients with MG who present with varying RNS results have provided a foundation for prospective growth in this area of research.

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#### **APPENDIX A**

#### **Myasthenia Gravis Fatigue Scale (MGFS)**

Following are <sup>a</sup> number of statements about fatigue related to Myasthenia Gravis. Respond to each statement by indicating how you generally feel when you experience fatigue. The following definition may help you: Fatigue is:

"a subjective experience ranging from tiredness to exhaustion and affects an individual'<sup>s</sup> ability to perform physical activity, mental activity, or both."

about the item.





\*Adapted from Eileen Hubsky and Jenean Sears.

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## **APPENDIX B**

# **Visual Analogue Scale (VAS)**

Directions: For the statement below, **provide a mark on** the **line** which best describes how you feel about the item.

1. My current level of fatigue is:

None at all

Extreme

2. In the past month, fatigue has affected my activities of daily living:

Not at all

Always

56

# **APPENDIX C**

# **Quantitative Myasthenia Gravis Score (QMG)**



 $\mathcal{L}^{\pm}$ 

 $\hat{\mathcal{A}}$ 

 $\label{eq:2.1} \frac{1}{\sqrt{2}}\int_{\mathbb{R}^3}\frac{1}{\sqrt{2}}\left(\frac{1}{\sqrt{2}}\right)^2\frac{1}{\sqrt{2}}\left(\frac{1}{\sqrt{2}}\right)^2\frac{1}{\sqrt{2}}\left(\frac{1}{\sqrt{2}}\right)^2.$ 

## **APPENDIX D**

# **Myasthenia Gravis- Activities of Daily Living Scale (MG-ADL)**

 $\overline{\phantom{a}}$ 




# The University of Western Ontario

APPENDIX E<br>
Office of Research Ethics<br>
The University of Western Ontario<br>
Room 00045 Dental Sciences Building, London, ON, Canada N6A 5C1<br>
Telephone: (519) 661-3036 Fax: (519) 850-2466 Email: ethics@uwo.ca<br>
Website: www. Room <sup>00045</sup> Dental Sciences Building, London, ON, Canada N6A <sup>501</sup> Telephone: (519) 661-3036 Fax: (519) 850-2466 Email: [ethics@uwo.ca](mailto:ethics@uwo.ca) Website: [www.uwo.ca/research/ethics](http://www.uwo.ca/research/ethics) **Review Number: <sup>13059</sup> Review Date:** February 6,2007 **Revision Number:**

## **Use of Human Subjects - Ethics Approval Notice**

**Principal Investigator: Dr. T.J. Doherty**

**Protocol Protocol Protocol Protocol Protocol Protocol Protocol Title: Quantitative evaluation of peripheral fatigue in myasthenia gravis patients** 

**Department and Institution:** Neurology, London Health Sciences Centre .

**Sponsor:**

**Ethics Approval Date: March 2,2007 Expiry Date:** June 30, <sup>2008</sup>

**Documents Reviewed and Approved:** UWO Protocol, Letter of Information and Consent -Control Subjects, Letter of ' Information and Consent -Subjects with Myasthenia Gravis, study advertisement

### **Documents Received** for **Information \_**

This is to notify you that The University of Western Ontario Research Ethics Board for Health Sciences Research Involving Human Subjects (HSRES) which is organized and operates according to the Tri-Council Policy Statement and the Health Canada/ICH Good Clinical Practice Practices: Consolidated Guidelines; and the applicable laws and regulations of Ontario has reviewed and granted full board approval to the above named research study on the approval date noted above. The membership of this REB also complies with the membership requirements for REB's as defined in Division 5 of the Food and Drug Regulations.

This approval shall remain valid until the expiry date noted above assuming timely and acceptable responses to the HSREB's periodic requests for surveillance and monitoring information. If you require an updated approval notice prior to that time you must request it using the UWO Updated Approval Request Form. •

During the course of the research, no deviations from, or changes to, the protocol or consent form may be initiated without prior written approval from the HSREB **except when necessary to** eliminate immediate hazards to the subject or when the change(s) involve only logistical or administrative aspects of the study (e.g. change of monitor, telephone number). Expedited review of minor change(s) in ongoing studies will be considered. Subjects must receive <sup>a</sup>copy of the signed information/consent documentation.

Investigators must promptly also report to the HSREB:

a) changes increasing the risk to the participant(s) and/or affecting significantly the conduct of the study;

b) all adverse and unexpected experiences or events that are both serious and unexpected;

c) new information that may adversely affect the safety of the subjects or the conduct of the study.

If these changes/adverse events require a change to the information/consent documentation, and/or recruitment advertisement, the newly revised information/consent documentation, and/or advertisement, must be submitted to this office for approval. change(s) involves only togetical or advertisement asspects of the study (e.g. change of monitor, telephone number).<br>Expedited review of minor change(s) in ongoing studies will be considered. Subjects must receive a copy o

Members of the HSREB who are named as investigators in research studies, or declare a conflict of interest, do not participate in discussion related to, nor vote on, such studies when they are presented to the HSREB.

— Chair of HSREB: Dr. John W. McDonald



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UWO HSREB Ethics Approval<br>2006-10-01 (HS-FB) 2006-10-01 *(HS-FB)* <sup>13059</sup> Page <sup>1</sup> of <sup>1</sup>



**The University of** Western Ontario

**Office of Research Ethics**<br>The University of Western Ontario<br>Room 00045 Dental Sciences Building, London, ON, Canada N6A 5C<br>Telephone: (519) 661-3036 Fax: (519) 850-2466 Email: ethics@uvo.c **Room <sup>00045</sup> Dental** Sciences Building, London, ON, Canada N6A 5C1 **Telephone: (519)** 661-3036 Fax: (519) 850-2466 Email: [ethics@uwo.ca](mailto:ethics@uwo.ca) **Website:** [www.uwo.ca/research/ethics](http://www.uwo.ca/research/ethics)

### **Use of Human Subjects - Ethics Approval Notice**



This is to notify you that The University of Western Ontario Research Ethics Board for Health Sciences Research Involving Human Subjects (HSREB) which is organized and operates according to the Tri-Council Policy Statement: Ethical Conduct of Research Involving Humans and the Health Canada/ICH Good Clinical Practice Practices: Consolidated Guidelines; and the applicable laws and regulations of Ontario has reviewed and granted approval to the above referenced revision(s) or amendment(s) on the approval date noted above. The membership of this REB also complies with the membership requirements for REB's as defined in Division <sup>5</sup> of the Food and Drug Regulations.

The ethics approval for this study shall remain valid-until the expiry date noted above assuming timely and acceptable responses to the HSREB's periodic requests for surveillance and monitoring information. If you require an updated approval notice prior to that time you must request it using the UWG Updated Approval Request Form.

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Members of the HSREB who are named as investigators in research studies, or declare a conflict of interest, do not participate in mewly revised information/consent documentation, and/or advertisement, must be submitted to this office for approval.<br>Members of the HSREB who are named as investigators in research studies, or declare a conflict of intere

> Chair of HSREB: Dr. John W. McDonald Deputy Chair: Susan Hoddinott



∕ .....Ethics Officer to Contact for Further Information .. Ethics Officer to Contact for Further Information<br>
Jennifer McEwen (jmcewen4@uwo.ca) | D Denise Grafton ([dgrafton@uwo.ca](mailto:dgrafton@uwo.ca)) | D Ethics Officer ([ethics@uwo.ca](mailto:ethics@uwo.ca))

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# Office of Research Ethics

The University of Western Ontario Room <sup>00045</sup> Dental Sciences Building, London, ON, Canada N6A <sup>501</sup> Room 00045 Dental Sciences Building, London, ON, Canada N6A 5C1<br>Telephone: (519) 661-3036 Fax: (519) 850-2466 Email: [ethics@uwo.ca](mailto:ethics@uwo.ca)<br>Website: [www.uwo.ca/research/ethics](http://www.uwo.ca/research/ethics)

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HanttMasayina kerakhimi<del>m kamamaa ka ka maabaa ka ma</del>

The ethics approval for this study shall remain valid until the expiry date noted above assuming timely and acceptable responses to the HSREB's periodic requests for surveillance and monitoring information. If you require an updated approval notice prior to that time you must request it using the UWO Updated Approval Request Form.

During the course of the research, no deviations from, or changes to, the protocol or consent form may be initiated without prior written approval from the HSREB except when necessary to eliminate immediate hazards to the subject or when the change(s) involve only logistical or administrative aspects of the study (e.g. change of monitor, telephone number). Expedited review of minor change(s) in ongoing studies will be considered. Subjects must receive <sup>a</sup> copy of the signed information/consent documentation.

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> Chair of HSREB: Dr. John W. McDonald Deputy Chair: Susan Heddinott



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